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Cancer remains a devastating condition that affects human health and quality of life

1-4. Immune compromised patients tend to be more susceptible to developing malignancy, including Kaposi's sarcoma (KS), primary effusion lymphoma (PEL), and multicentric Castleman's disease<sup>5,6</sup>. Such conditions are tightly linked with Kaposi's sarcoma-associated herpesvirus (KSHV, also known as Human Herpesvirus-8 (HHV-8)). KSHV, a gamma-2 herpesvirus, is an oncogenic virus with a double-stranded deoxyribonucleic acid (DNA) genome<sup>6-9</sup>. KSHV infection is primarily latent, including in tumor cells<sup>6,10</sup>. During latent infection, the virus persists as a multiple copy, extrachromosomal episome<sup>6</sup>. The latency-associated nuclear antigen (LANA) is one of several genes expressed

ension) two-dimensional (2-D) cultures. 2-D cultures lack many features of the native  
As a result, many *in vivo* physiologic properties that may be crucial to defining a cell's  
n, such as signaling through certain pathways (e.g.,

Various 3-D culturing techniques (*e.g.*, hanging drop, microfluidic systems, bioprinting, assembly, spinner flasks, and rotary system) have been successfully used to generate 3-D tumor models<sup>19–33</sup>. For example, hanging drop approach has been increasingly used to generate 3-D models due its simplicity; however, it is still challenging to use this method to provide long-term cultures. The rotary system and the spinner flasks are suitable for long-term cultures; however, they are unable to generate consistently sized 3-D constructs and require special equipment<sup>34</sup>. Further, bioprinting and assembly are fabrication techniques that may require a subsequent culturing system (*i.e.*, bioreactors) to grow and mature cells<sup>19,35</sup>. While microfluidic systems have shown promise in 3-D culture, high fluid flow induced-shear stress can affect cell physiology<sup>22</sup>. A detailed description of advantages and disadvantages of each technique is shown in Supplementary Information (SI) Table S1. Although such techniques have been successfully applied for tissue engineering and regenerative medicine applications (*e.g.*, generation of 3-D models of stem cells<sup>36</sup> and hepatocytes<sup>37,38</sup>), only a few were utilized to culture virus-infected tumor cells<sup>18</sup>. In one report, a 3-D *in vitro* model for KSHV infection was developed using spheroids embedded in clotted fibrin gel<sup>15</sup>.

and 300  $\mu\text{m}$  microwells at the same location. Thus, based on this simulation data and the size distribution results (Fig. 1b), the 450  $\mu\text{m}$  microwell platform was chosen to be the basis of our subsequent experiments.

To evaluate the feasibility of growing virus-infected cells in 3-D, KSHV-infected BJAB and uninfected (control) BJAB cells were seeded into the microwells and cultured both with and without puromycin selection (Figs 1c and 3). The cells were seeded at a low-density ( $\leq 100$  cells/microwell) to allow for direct observation and monitoring of proliferation during the experiment. Although precise control over the number of seeded cells per microwell is a challenge, it was clear that increasing the cell concentration when seeding the microwells resulted in increased numbers of cells settling into microwells<sup>45</sup>. The cell occupancy in a microwell array has been previously investigated both theoretically and experimentally<sup>46,47</sup>. In our microwell system, as the microwell size is much larger than the cell size, the cells already present in a given microwell will not affect addition of new cells to that same microwell. The probability ( $f$ ) of a microwell containing  $n$  cells can be described by the equation of Poisson distribution as below,

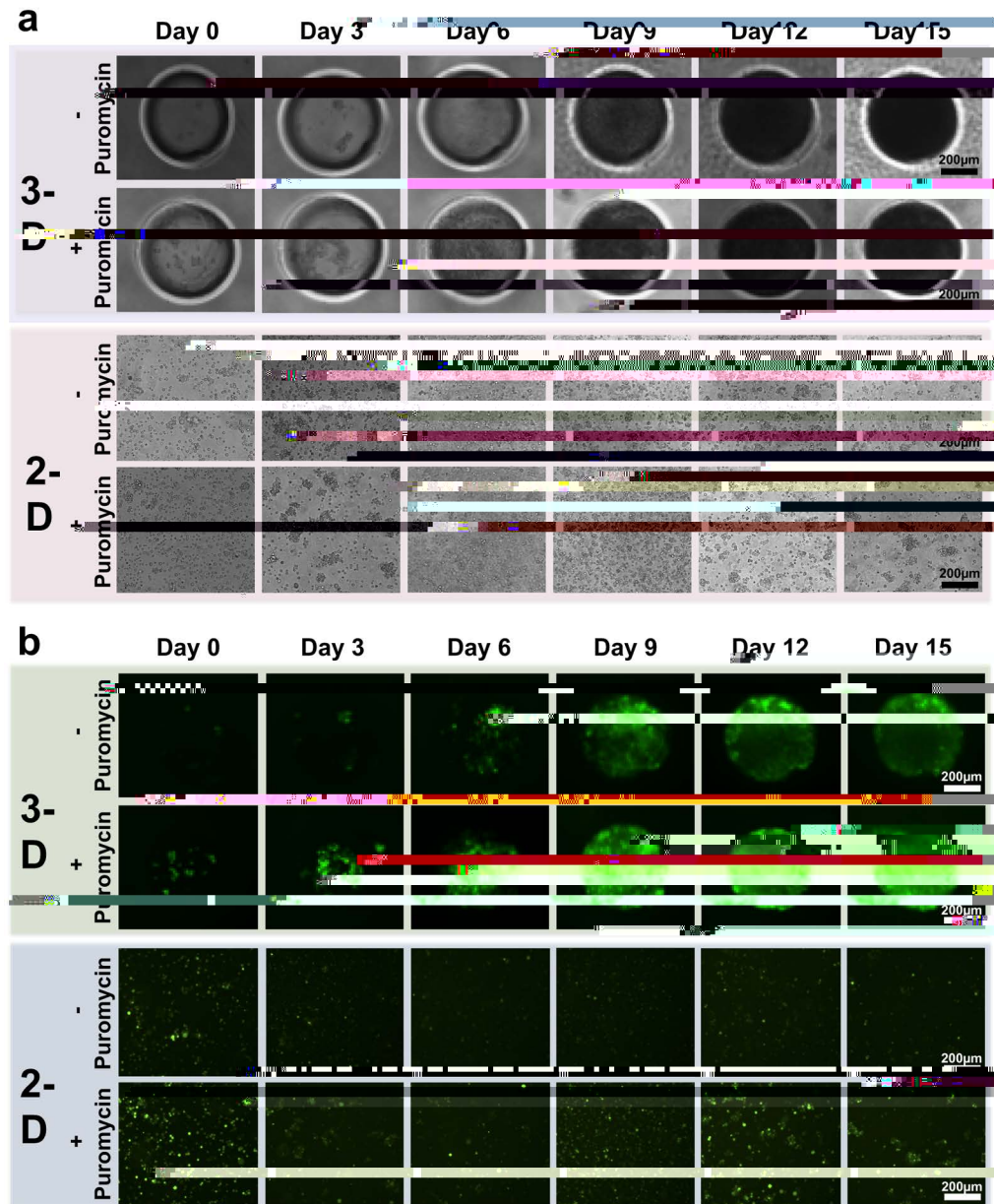
$$f(n; \lambda) = \frac{\lambda^n e^{-\lambda}}{n!} \quad (3)$$

where  $\lambda$  is the average number of cells per microwell area on the glass slide. As  $\lambda$  increases the Poisson distribution approaches the Gaussian form. The peak or maximum of the Poisson distribution corresponds to the mean ( $\lambda$ ). Thus, the average cell number in microwells can be modulated by the cell seeding density on the glass slide.

Once cells settle inside the microwells, they do not displace during exchange of cell culture media. The cells can be harvested without compromising their viability<sup>48</sup> by tilting the platform at 45°.

grow in aggregates determined by the size and shapes of the constructed microwells, and with cell-to-cell contact occurring in three dimensions.

Subsequent to cell seeding, a series of bright field photomicrographs were obtained of each microwell for 15 days. The results demonstrated that there was no significant difference in the proliferation rate between KSHV-infected BJAB cells cultured with or without puromycin selection (Figs 3a and 4a). This result is expected since the recombinant KSHV expresses the puromycin resistance gene. Proliferating cells grew efficiently until they filled the entire microwell (at around day 15), and subsequently began to spill out from the microwells (SI Figure 3). This cell outgrowth occurs due to the non-adhesive properties of PEG, and results in some non-ho12.4(n)o Tc -0.8rs cell mTc -0.8-8.7(de)4.3(l)13.(s a)9.2( )6.3(er d)-2.8(a)18.3(y 15. )4.3(e ini)12.3(t)-4.7(i)-2. summarizes the volumTc -0es of the 3-D models that were ge Tc -0erated rsing di erent sizes of microwells. The size of the



**Figure 3.** KSHV infected BJAB cell maintenance in 3-D 450 μm microcell 2-D culture. (a) Bright field photomicrographs of infected BJAB cells grown for 15 days. Images were taken at 3-day intervals, beginning with the day of seeding. Scale bars indicating 200 μm are shown. (b) Fluorescent photomicrographs of infected BJAB cells grown for 15 days. Expression of GFP (green) by the infected cells, which were cultured in 2-D or 3-D, indicates KSHV infection. Scale bars represent 200 μm. In the absence of puromycin selection, less fluorescence was observed over time in cells in 2-D and 3-D culture due to loss of KSHV infection. This is a representative figure for the subsequent quantification figure (i.e., Fig. 4). Scale bars indicating 200 μm are shown.

~2–3 fold more LANA dots present in infected cells in 3-D compared to 2-D culture (Fig. 5a), indicating a higher KSHV genome copy number since each LANA dot corresponds to a viral genome. Consistent with this finding, both in the presence or absence of puromycin, the 3-D cultures had much brighter fluorescence compared to the 2-D cultures (Figs 3 and 5). We also investigated lytic reactivation at 15 days by detecting the KSHV lytic protein product, ORF59 (Fig. 5b). Reactivation from BJAB-KSHV cells was very inefficient, and even after induction with 12-O-tetradecanoyl phorbol-13-acetate (TPA) and sodium butyrate fewer than 1% of cells expressed ORF59 (data not shown). However, we observed that ~3 fold more cells expressed ORF59 in 3-D versus 2-D culture in the presence of puromycin as there were ~15 ORF59 expressing cells in 3-D compared to ~5 ORF59 expressing cells in 2-D (with similar numbers of total cells plated per slide). In the absence of puromycin, fewer cells underwent reactivation in 3-D, perhaps related to lower episome copy number, but there still appeared to be more ORF59

expressing cells compared to 2-D culture without puromycin. These findings of increased episome copy number and increased lytic reactivation are similar to previous observations made by Cheng *et al.* when KSHV infected primary endothelial cells were grown in 3-D after embedding spheroids in fibrin gel<sup>15</sup>. Therefore, it is likely that autocrine and paracrine signaling in the 3-D microenvironment contributes to enhanced infection with higher viral genome copy per cell and a higher rate of lytic reactivation, perhaps more similar to conditions present *in vivo*<sup>49,50</sup>.

In this study, we report the ability to culture human KSHV-infected BJAB cells in 3-D using a microwell format. The use of microwell-based culture for the purpose of growing virus-associated tumor cells in 3-D has not been well studied or applied. One challenge of this concept is the difficulty to extend the culture for a longer period (>3 weeks) of time without the detachment of the PEG hydrogel from the TMSPMA coated slides as a result of the weakening of the attachment between the PEG microwells and the glass. However, stability of the PEG attachment can be enhanced by etching the glass surface with a mixture of sulfuric acid and hydrogen peroxide (piranha etch)<sup>51</sup> as well as treating the surface with oxygen plasma to form an oxygen-rich layer<sup>52,53</sup>. Furthermore, the present method has the potential to allow further investigation of the recovered KSHV-infected BJAB cells after long term culture, such as flow cytometry or polymerase chain reaction. Moreover, this approach would provide the basis for future work to further investigate the biology of KSHV infected cells grown in 3-D, including potential effects on cytokine production. In addition, investigation of other infected cell types, such as endothelial cells, would be a logical next step for the applications of this approach. This innovative platform can also be used to

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Here, we demonstrate the ability to grow KSHV-infected human BJAB cells in 3-D cultures. The cells were cultured in PEG-based 3-D microwell array system for up to 15 days. Compared with culture in 2-D, cells in 3-D had more nuclear LANA dots, indicating a higher KSHV genome copy number, and cells in 3-D also underwent lytic reactivation at a higher rate. The 3-D microwell array system has the potential to improve cell culture strategies and allow for better-controlled studies for drug discovery and experimental biology.

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/š<sup>o</sup> @š<sup>o</sup> ✕<sup>a</sup> «š<sup>-</sup> ! ' ! «Ÿ<sup>-</sup> Poly(dimethylsiloxane) (PDMS) molds were fabricated by thoroughly mixing (10:1) of elastomer and curing agent (SYLGARD 184 Silicone Elastomer Kit; Sigma). The mixture was poured on a silicon master patterned with SU-8 photoresist, degassed in a vacuum chamber for 30 minutes, and then allowed to cure at 70 °C for 2 hours. The silicon master (positive structure) has circular depressions, which were replicated into PDMS (negative structure) for the following fabrication steps. Three different silicon masters were used to prepare different sizes of PDMS molds with cylindrical protrusions of: 150 μm (diameter) 9





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